

Abstract

Background: The present study investigated the effects of a 10-day transcranial magnetic stimulation (TMS) protocol on the motor cortex excitability (MCE) and on the motor cortex plasticity (MCP) in healthy subjects. The study was designed to test the hypothesis that TMS can induce long-term potentiation (LTP) of the motor cortex excitability.

Methods: A total of 15 healthy subjects participated in the study. The subjects were divided into two groups: a control group (n = 7) and an experimental group (n = 8). The experimental group received a 10-day TMS protocol, while the control group received a sham TMS protocol. The MCE and MCP were measured before and after the TMS protocol.

Results: The results showed that the TMS protocol significantly increased the MCE and MCP in the experimental group compared to the control group. The increase in MCE was maintained for at least 24 hours after the TMS protocol.

Conclusions: The results of the present study suggest that a 10-day TMS protocol can induce LTP of the motor cortex excitability in healthy subjects.

Keywords: Transcranial magnetic stimulation; Motor cortex excitability; Motor cortex plasticity; Long-term potentiation.

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ABSTRACT

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2. Methods

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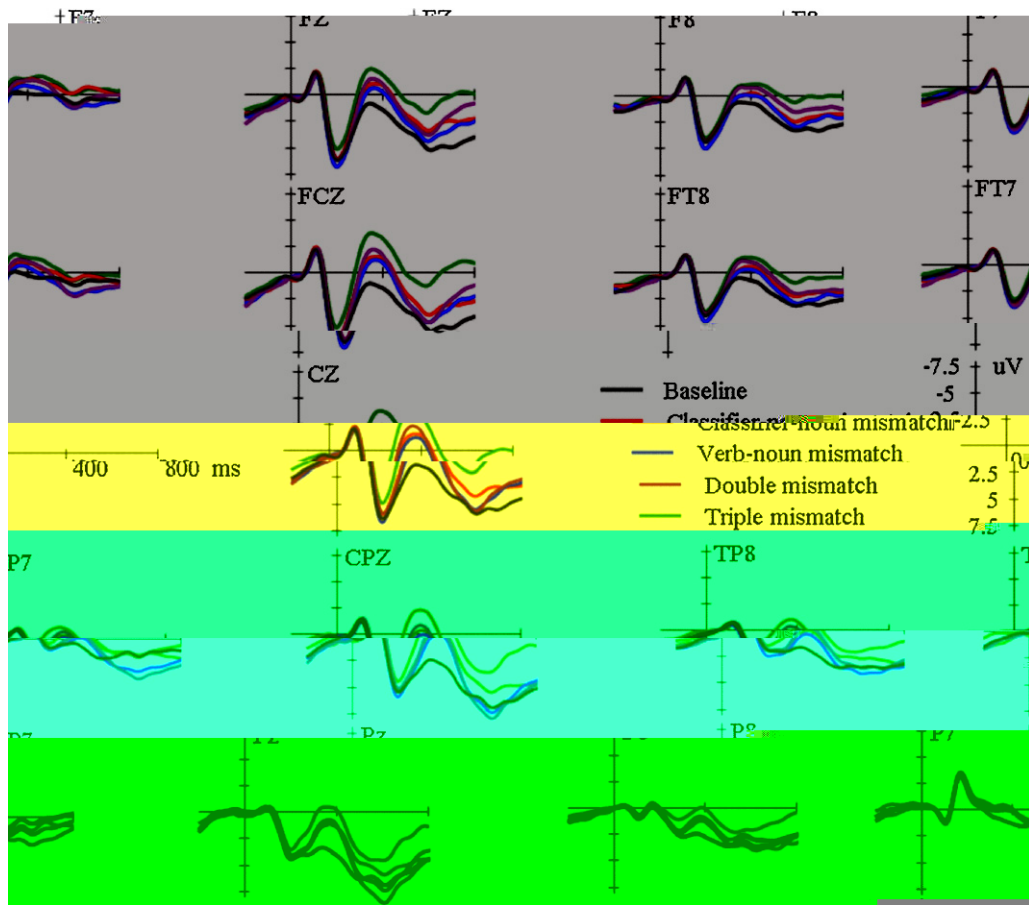


Fig. 2. ERP waveforms for mismatch conditions. The figure is a 3x4 grid of plots showing voltage (uV) over time (ms) for different electrode sites (F7, FZ, F8, F9, FCZ, FT8, FT7, CZ, P7, CPZ, TP8, P8, P9, Pz, P7, P8, P9). The legend indicates: Baseline (black), Classifier-noun mismatch (red), Verb-noun mismatch (blue), Double mismatch (orange), and Triple mismatch (green). A color bar on the right indicates voltage levels from -7.5 to 7.5 uV. A time scale bar at the top indicates 400 and 800 ms.

ss fi $(-0.53 \mu V)$ ss fi $F(1, 25) = 5.09, p < 0.05$ ss fi $F(1, 25) = 3.97, p < 0.05$ ss fi $F(1, 25) = 4.17, p < 0.05$

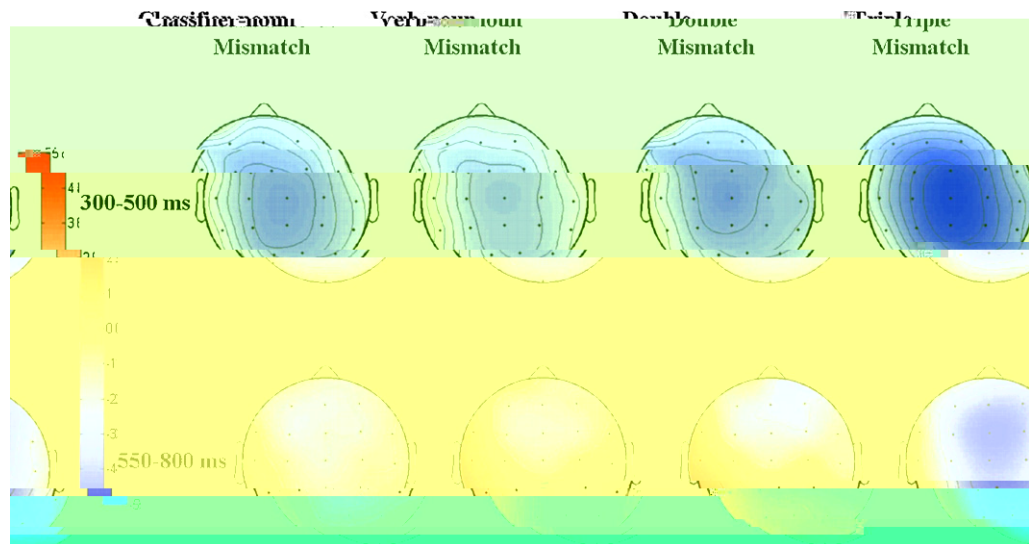


Fig. 3. Topographic maps of ERP waveforms for mismatch conditions. The figure shows four columns of topographic maps for Classifier-noun Mismatch, Verb-noun Mismatch, Double Mismatch, and Triple Mismatch. The maps are arranged in a 2x4 grid, with the top row showing the 300-500 ms time window and the bottom row showing the 550-800 ms time window. A color bar on the left indicates voltage levels from -5 to 5 uV.

Table 3

Condition	s				ss fi				s				s			
	F	p	ϵ		F	p	ϵ		F	p	ϵ		F	p	ϵ	
—	1,25	39.73	<0.001	1.00	1,25	11.13	<0.005	1.00	1,25	15.51	<0.005	1.00	1,25	6.61	<0.05	1.00
×	4,100	7.87	<0.005	0.49	4,100	2.16	0.12	0.54	4,100	3.54	<0.05	0.59	4,100	2.21	0.12	0.53
—	1,25	39.42	<0.001	1.00	1,25	10.61	<0.005	1.00	1,25	12.44	<0.005	1.00	1,25	3.42	0.08	1.00
×	1,25	15.21	<0.005	1.00	1,25	8.13	<0.01	1.00	1,25	3.19	0.09	1.00	1,25	1.75	0.20	1.00
×	1,25	0.12	0.73	1.00	1,25	0.10	0.75	1.00	1,25	0.15	0.70	1.00	1,25	0.89	0.35	1.00
×	1,25	4.33	<0.05	1.00	1,25	2.00	0.17	1.00	1,25	3.90	0.06	1.00	1,25	3.57	0.07	1.00

Note: s = s; ss fi = ss fi; s = s; s = s.

Table 4

Condition	s				ss fi				s				s			
	F	p	ϵ		F	p	ϵ		F	p	ϵ		F	p	ϵ	
—	1,25	26.46	<0.001	1.00	1,25	13.66	<0.005	1.00	1,25	29.23	<0.001	1.00	1,25	21.53	<0.001	1.00
×	4,100	10.69	<0.001	0.62	4,100	3.34	<0.05	0.56	4,100	2.51	0.09	0.56	4,100	13.25	<0.001	0.65
—	1,25	24.03	<0.001	1.00	1,25	10.39	<0.005	1.00	1,25	28.99	<0.001	1.00	1,25	19.10	<0.001	1.00
×	1,25	20.33	<0.001	1.00	1,25	18.18	<0.001	1.00	1,25	8.36	<0.01	1.00	1,25	0.24	0.63	1.00
×	1,25	10.36	<0.005	1.00	1,25	0.01	0.92	1.00	1,25	0.01	0.99	1.00	1,25	14.86	<0.005	1.00
×	1,25	0.16	0.69	1.00	1,25	1.56	0.22	1.00	1,25	0.37	0.55	1.00	1,25	0.04	0.85	1.00

Note: s = s; ss fi = ss fi; s = s; s = s.

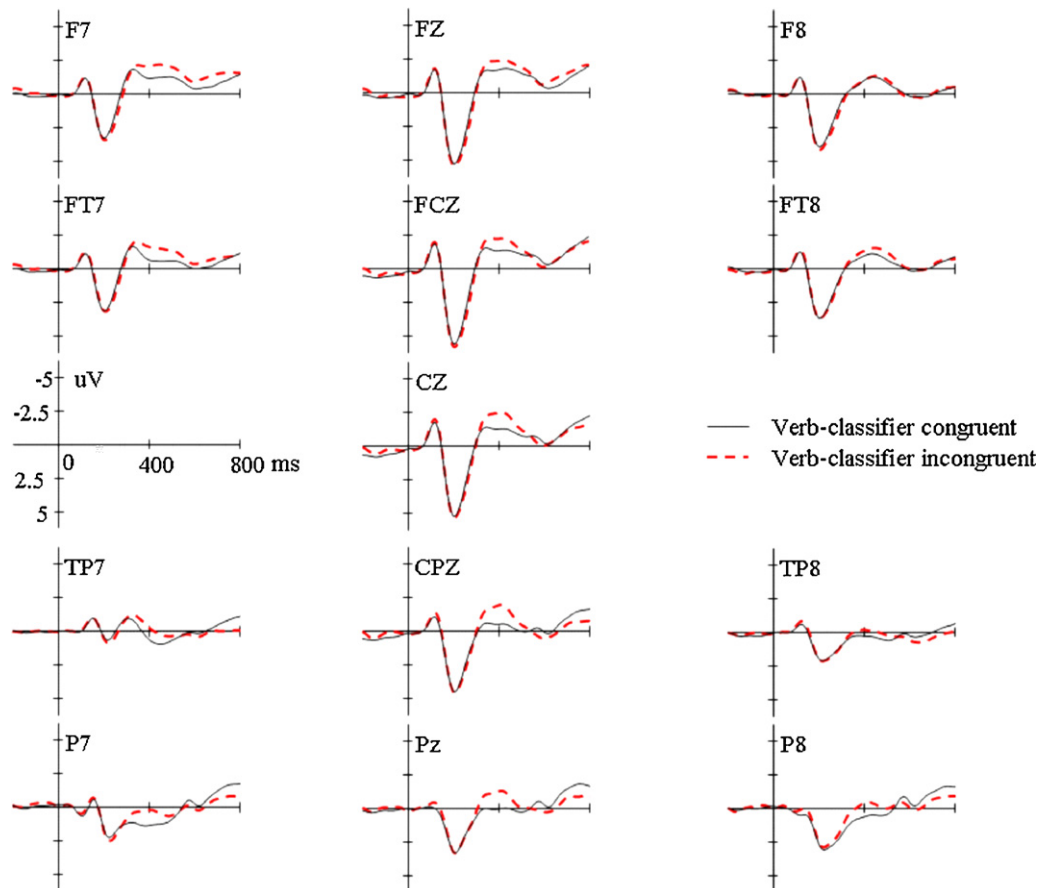


Fig. 4. ERP waveforms for Verb-classifier congruent (solid line) and incongruent (dashed line) conditions across various electrode sites (F7, FZ, F8, FT7, FCZ, FT8, TP7, CPZ, TP8, P7, Pz, P8). The y-axis represents voltage in uV (ranging from -5 to 5) and the x-axis represents time in ms (ranging from 0 to 800).

4. Discussion

The proposed method is a novel approach for the classification of EEG signals. It is based on the combination of the wavelet transform and the support vector machine (SVM). The wavelet transform is used to extract the features from the EEG signals, and the SVM is used to classify the features. The results show that the proposed method is effective in the classification of EEG signals. The accuracy of the proposed method is higher than that of the traditional methods. The proposed method is also robust to the noise and the non-stationary signals. The proposed method is suitable for the real-time classification of EEG signals. The proposed method is also suitable for the classification of EEG signals in the field of brain-computer interface (BCI).

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